

Value of Black-blood MR Angiography Generated from **Vessel Wall Imaging in the Assessment of Stented Intracranial Arteries**

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Background

Intracranial stents are often used to assist embolization of widenecked aneurysms (1, 2). Although the long-term benefit has been denied, stenting may still be beneficial in some patients with intracranial artery stenosis in combination with percutaneous transluminal angioplasty (3, 4). Stents cause endothelial hyperplasia or thrombosis. For the assessment of stented intracranial arteries, DSA, 3D-TOF MRA and CTA have been employed. However, their clinical value is limited due to invasiveness and/or artifacts including susceptibility artifacts, radiofrequency shielding and turbulent/laminar flow (6, 7).

Purpose

For intracranial vessel wall imaging (VWI), we have used a SPACE (sampling perfection with application optimized contrast using different flip angle evolution; Siemens Healthineers) sequence based on a fast spin-echo technique with variable flip angle refocusing pulses. Therefore, we hypothesized that VWI may be useful for the accurate evaluation of the stented artery. In this study, we comparatively evaluated the depiction of stented artery between conventional 3D-TOF MRA and black-blood MRA (BB-MRA) generated from VWI data obtained using the SPACE sequence in order to prove the hypothesis.

Materials and Methods

Imaging

✓ 3T MR scanner (Verio, Siemens Healthineers)

	3D-TOF MRA	VWI and BB-MRA
Sequence	3D FFE	SPACE
Receiver coil	32ch head coil	32ch head coil
Repetition time/Echo time	23/3.95 msec	540/11 msec
Matrix	318×448	270×256
Field of view	200	240
Slice thickness/number	0.6 mm/120	0.9 mm/192
Scan time	6 min 30 sec	7 min 35 sec

Results (cont'd)

(2) Vessel diameter

Significant difference was present in the relative diameter indexes (DIs) between 3D-TOF and BB-MRA (0.58 vs. 0.96, P<0.01). On 3D-TOF MRA, the diameter of the stented artery was smaller than that of the normal artery in all cases (the average ratio = 0.56). However, there was no difference in the diameter on BB-MRA (the average ratio = 0.94).

(3) Visual assessment

There was significant difference between 3D-TOF MRA and BB-MRA (1.0 *vs.* 3.0, P<0.05).

On 3D-TOF MRA, the flow signal tended to be discontinuous or heterogeneous. On the BB-MRA, the flow signal was homogeneous and continuous in all cases.

Representative Case (68-y.o. female after stent-assisted coil embolization for a left MCA aneurysm)



3D-TOF MRA

DSA

On 3D-TOF MRA, left M1 seems to show irregularity and stenosis. On BB-MRA, however, the M1 is apparently patent. DSA shows patent M1 lumen that is well corresponding with BB-MRA.

Discussion

The CR of the stented artery was significantly higher than that of the normal artery on BB-MRA than on 3D-TOF MRA. Similarly, visual assessment showed that BB-MRA is better than 3D-TOF MRA in signal homogeneity and continuity. These are probably due to signal loss of the stented artery caused by susceptibility artifacts in 3D-TOF MRA using a gradient-echo sequence, while BB-MRA is free from such artifacts as it uses a spin-echo sequence. On 3D-TOF MRA, shielding effects, which induce currents in the stent wall, reportedly more affects signal of the stented artery than susceptibility artifacts (5). In a study that evaluated difference in signal loss among several kinds of stents, LVIS stent has been reported to show the minimal degree (6). Our group previously performed a similar study in clinical cases and it showed that, although difference was statistically insignificant, the CR of LVIC stent tended to be low compared with Neuroform atlas (7). This suggests that geometry and orientation of stents affect susceptibility artifacts leading to more signal loss than that caused by shielding effects. Anyway, judging from our results of the assessment of relative DI, BB-MRA seems to be more accurate than 3D-TOF MRA in assessing lumen of the stented arteries. Although not evaluated in the present study, source images of VWI before performing minIP could also be informative.



Image analysis

(1) Contrast ratio

- \checkmark Signal intensity (SI) of the central part of stented artery, the normal artery proximal to the stent and the normal white matter were measured on source images.
- ✓ The contrast ratio (CR) = (SI_{white matter} SI_{stented artery}) / (SI white matter + SI_{proximal artery})

(2) Vessel diameter

- \checkmark For both stented artery and normal artery proximal to the stent, the profiling curve was obtained in cross section for each artery on source images using the ImageJ software by manual plotting. The full width at half maximum (FWHM) was regarded as the diameter.
- ✓ The relative diameter index (DI) = the diameter (stented artery) / (normal artery proximal to the stent)

(3) Visual assessment

 \checkmark We visually assessed depiction of the artery at the poststenting site using the following four-grade visual assessment score.

Score Visual assessment of the depiction at the stented artery

- Complete signal loss 0
- Discontinuous flow signal 1
- Continuous and heterogeneous flow signal 2
- 3 Continuous and homogeneous flow signal

Results

(1) Contrast ratio

On 3D-TOF MRA, the CR of the stented artery was significantly lower than that of the normal artery (0.43 vs. 0.67, P<0.05). On BB-MRA, there was no significant difference in the CR for both stented artery and normal artery (0.90 vs. 0.90, P=0.926).

Conclusion

BB-MRA generated from VWI could be useful for the follow-up study of stent-assisted treatment of intracranial arterial diseases.

References

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